

Package: PhysioECG (via r-universe)

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Title ECG Analysis Functions for PhysioExperiment Objects

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Description Provides electrocardiography (ECG) analysis functions for PhysioExperiment objects. Includes R-peak detection (adaptive Pan-Tompkins), RR interval computation, HRV time-domain metrics (SDNN, RMSSD, pNN50), HRV frequency-domain analysis (VLF, LF, HF power), nonlinear HRV (Poincare, Sample Entropy, DFA), ECG morphology analysis (QRS boundaries, QT/QTc intervals), and signal quality assessment with ectopic beat correction.

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ecgBaselineCorrect	<i>Correct Baseline Wander in ECG Signals</i>
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Description

Removes low-frequency baseline drift from ECG data using either a high-pass moving-average subtraction or a running-median subtraction.

Usage

```
ecgBaselineCorrect(
  x,
  method = c("highpass", "median"),
  cutoff = 0.5,
  assay_name = NULL,
  output_assay = "baseline_corrected"
)
```

Arguments

x	A <code>PhysioExperiment</code> object with ECG data.
method	Correction method: "highpass" (default) subtracts a moving average; "median" subtracts a running median.
cutoff	Approximate cutoff frequency in Hz (default: 0.5). Controls the window size of the moving average or median filter.

assay_name Name of the input assay. If NULL the default assay is used.
 output_assay Name of the assay in which to store the corrected signal (default: "baseline_corrected").

Value

A PhysioExperiment with the corrected signal stored in output_assay.

References

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

See Also

[ecgSignalQuality](#) for signal quality assessment, [ecgDetectRpeaks](#) for R-peak detection, [ecgQualityCheck](#) for ectopic beat detection.

ecgDelineate	<i>Delineate ECG Waveform Morphology</i>
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Description

For each detected R-peak, identifies QRS complex boundaries (onset and offset) and P-wave and T-wave peaks. QRS boundaries are detected using a gradient-based search from the R-peak, while P and T waves are found as local maxima in physiologically plausible time windows.

Usage

```
ecgDelineate(x, peaks, assay_name = NULL)
```

Arguments

x A PhysioExperiment object with ECG data.
 peaks A data.frame of detected R-peaks as returned by [ecgDetectRpeaks](#), with columns channel and sample.
 assay_name Name of the assay to use. If NULL, the default assay is used.

Value

A data.frame with one row per beat and the following columns:

channel Integer channel index (1-based).
beat Integer beat number within the channel (1-based).
r_peak Sample index of the R-peak.
qrs_onset Sample index of QRS complex onset.
qrs_offset Sample index of QRS complex offset (J-point).

qrs_duration_ms QRS complex duration in milliseconds.
p_peak Sample index of P-wave peak, or NA if not found in the search window (300–80 ms before R-peak).
t_peak Sample index of T-wave peak, or NA if not found in the search window (80–500 ms after R-peak).
t_end Sample index of T-wave end estimated by tangent-intercept method, or NA if T-wave not found.

Returns a zero-row data.frame with the same column structure if no beats are delineated.

References

Goldberger, A.L., et al. (2000). "PhysioBank, PhysioToolkit, and PhysioNet: Components of a new research resource for complex physiologic signals." *Circulation*, 101(23), e215–e220. doi:10.1161/01.CIR.101.23.e215

See Also

[ecgDetectRpeaks](#) for R-peak detection, [ecgIntervals](#) for computing clinical ECG intervals from delineation results, [ecgSignalQuality](#) for signal quality assessment.

Examples

```
## Not run:
pe <- make_ecg(n_time = 5000, sr = 500, heart_rate = 72)
peaks <- ecgDetectRpeaks(pe)
delin <- ecgDelineate(pe, peaks)
head(delin)

## End(Not run)
```

ecgDetectRpeaks

Detect R-Peaks in ECG Signal Using Pan-Tompkins Algorithm

Description

Identifies R-peaks in ECG data using an adaptive dual-threshold Pan-Tompkins detector. The algorithm applies bandpass filtering (5-15 Hz), differentiation, squaring, and moving-window integration followed by adaptive thresholding with running signal and noise level estimates. Automatically detects and handles inverted ECG signals.

Usage

```
ecgDetectRpeaks(
  x,
  method = "pan_tompkins",
  threshold_factor = 0.6,
  refractory_ms = 200,
  assay_name = NULL
)
```

Arguments

x	A <code>PhysioExperiment</code> object with ECG data.
method	Detection method. Currently only "pan_tompkins" is supported.
threshold_factor	Fraction of the peak integrated signal used as the detection threshold (default: 0.6).
refractory_ms	Refractory period in milliseconds. No two peaks can be closer than this (default: 200).
assay_name	Name of the assay to use. If NULL, the default assay is used.

Value

A `data.frame` with one row per detected R-peak and the following columns:

channel Integer channel index (1-based).

sample Integer sample index of the R-peak within the assay matrix.

time_sec Time of the R-peak in seconds from signal onset.

amplitude Amplitude of the raw signal at the R-peak location (in original units, not inverted).

Returns a zero-row `data.frame` with the same column structure if no peaks are detected.

References

Pan, J. & Tompkins, W.J. (1985). "A real-time QRS detection algorithm." *IEEE Transactions on Biomedical Engineering*, 32(3), 230–236. doi:[10.1109/TBME.1985.325532](https://doi.org/10.1109/TBME.1985.325532)

See Also

[ecgRRintervals](#) for computing RR intervals from detected peaks, [ecgDelineate](#) for full waveform morphology analysis, [ecgSignalQuality](#) for signal quality assessment.

Examples

```
## Not run:
pe <- make_ecg(n_time = 5000, sr = 500, heart_rate = 72)
peaks <- ecgDetectRpeaks(pe)
head(peaks)

## End(Not run)
```

ecgDFA

Detrended Fluctuation Analysis of RR Intervals

Description

Performs detrended fluctuation analysis (DFA) on RR interval data to characterize fractal scaling properties. Computes alpha1 (short-range correlations, 4–16 beats) and alpha2 (long-range correlations, 16–64 beats).

Usage

```
ecgDFA(rr, short_range = c(4, 16), long_range = c(16, 64))
```

Arguments

rr	A data.frame with columns channel, rr_ms, and time_sec, as returned by ecgRRintervals .
short_range	Numeric vector of length 2 defining the scale range (in beats) for alpha1 (default: c(4, 16)).
long_range	Numeric vector of length 2 defining the scale range (in beats) for alpha2 (default: c(16, 64)).

Value

A data.frame with one row per channel and the following columns:

channel Integer channel index.

alpha1 Short-range scaling exponent. Values near 1.0 indicate fractal-like (healthy) correlations; values near 0.5 indicate uncorrelated (random) behavior; values near 1.5 suggest Brownian noise. NA if the series is too short.

alpha2 Long-range scaling exponent with the same interpretation as alpha1 but over larger time scales. NA if the series is too short.

References

Peng, C.-K., et al. (1994). "Mosaic organization of DNA nucleotides." *Physical Review E*, 49(2), 1685–1689. doi:[10.1103/PhysRevE.49.1685](https://doi.org/10.1103/PhysRevE.49.1685)

See Also

[ecgHRVnonlinear](#) for the combined nonlinear analysis wrapper, [ecgSampleEntropy](#) for sample entropy, [ecgHRVpoincare](#) for Poincare plot descriptors.

Description

Computes heart rate variability frequency-domain metrics from RR interval data using Welch's method or Lomb-Scargle periodogram.

Usage

```
ecgHRVfreq(
  rr,
  method = c("welch", "lomb"),
  vlf_band = c(0.003, 0.04),
  lf_band = c(0.04, 0.15),
  hf_band = c(0.15, 0.4)
)
```

Arguments

<code>rr</code>	A data.frame with columns <code>channel</code> , <code>rr_ms</code> , and <code>time_sec</code> , as returned by ecgRRintervals .
<code>method</code>	Spectral estimation method: "welch" (default) for uniformly resampled FFT-based PSD, or "lomb" for Lomb-Scargle periodogram on unevenly sampled data.
<code>vlf_band</code>	Numeric vector of length 2 defining VLF band in Hz (default: <code>c(0.003, 0.04)</code>).
<code>lf_band</code>	Numeric vector of length 2 defining LF band in Hz (default: <code>c(0.04, 0.15)</code>).
<code>hf_band</code>	Numeric vector of length 2 defining HF band in Hz (default: <code>c(0.15, 0.4)</code>).

Value

A data.frame with one row per channel and the following columns:

channel Integer channel index.

vlf Absolute power in the very-low-frequency band (ms^2).

lf Absolute power in the low-frequency band (ms^2), associated with sympathetic and parasympathetic modulation.

hf Absolute power in the high-frequency band (ms^2), associated with parasympathetic (vagal) modulation.

lf_hf_ratio Ratio of LF to HF power, or NA if HF power is zero.

total_power Sum of VLF, LF, and HF power (ms^2).

References

Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996). "Heart rate variability: Standards of measurement, physiological interpretation and clinical use." *Circulation*, 93(5), 1043–1065.

See Also

[ecgRRintervals](#) for computing RR intervals, [ecgHRVtime](#) for time-domain HRV metrics, [ecgHRVnonlinear](#) for nonlinear HRV analysis, [ecgRRcorrect](#) for ectopic beat correction before analysis.

Examples

```
n <- 300
time_sec <- cumsum(rep(0.85, n))
rr_ms <- 850 + 30 * sin(2 * pi * 0.1 * time_sec)
rr <- data.frame(channel = rep(1L, n), rr_ms = rr_ms, time_sec = time_sec)
result <- ecgHRVfreq(rr, method = "welch")
```

ecgHRVnonlinear

Nonlinear HRV Analysis (Convenience Wrapper)

Description

Computes all nonlinear HRV metrics by calling [ecgHRVpoincare](#), [ecgSampleEntropy](#), and [ecgDFA](#), and merging the results into a single data.frame.

Usage

```
ecgHRVnonlinear(
  rr,
  m = 2L,
  r_factor = 0.2,
  short_range = c(4, 16),
  long_range = c(16, 64)
)
```

Arguments

rr	A data.frame with columns channel, rr_ms, and time_sec, as returned by ecgRRintervals .
m	Embedding dimension for sample entropy (default: 2).
r_factor	Tolerance factor for sample entropy (default: 0.2).
short_range	Scale range for DFA alpha1 (default: c(4, 16)).
long_range	Scale range for DFA alpha2 (default: c(16, 64)).

Value

A data.frame with columns: channel, sd1, sd2, sd1_sd2_ratio, sample_entropy, m, r, alpha1, alpha2.

References

Shaffer, F. & Ginsberg, J.P. (2017). "An overview of heart rate variability metrics and norms." *Frontiers in Public Health*, 5, 258. doi:10.3389/fpubh.2017.00258

Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996). "Heart rate variability: Standards of measurement, physiological interpretation and clinical use." *Circulation*, 93(5), 1043–1065.

See Also

[ecgHRVpoincare](#) for Poincare plot descriptors, [ecgSampleEntropy](#) for sample entropy, [ecgDFA](#) for detrended fluctuation analysis, [ecgHRVtime](#) for time-domain HRV metrics, [ecgHRVfreq](#) for frequency-domain HRV analysis.

ecgHRVpoincare

Poincare Plot Descriptors for HRV Analysis

Description

Computes Poincare plot descriptors (SD1, SD2, SD1/SD2 ratio) from RR interval data. SD1 reflects short-term variability (perpendicular to the identity line), while SD2 reflects long-term variability (along the identity line).

Usage

```
ecgHRVpoincare(rr)
```

Arguments

rr A data.frame with columns channel, rr_ms, and time_sec, as returned by [ecgRRintervals](#).

Value

A data.frame with one row per channel and the following columns:

channel Integer channel index.

sd1 Standard deviation perpendicular to the identity line (ms), reflecting beat-to-beat (short-term) variability.

sd2 Standard deviation along the identity line (ms), reflecting long-term variability.

sd1_sd2_ratio Ratio of SD1 to SD2, or NA if SD2 is zero.

References

Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996). "Heart rate variability: Standards of measurement, physiological interpretation and clinical use." *Circulation*, 93(5), 1043–1065.

See Also

[ecgHRVnonlinear](#) for the combined nonlinear analysis wrapper, [ecgSampleEntropy](#) for sample entropy, [ecgDFA](#) for detrended fluctuation analysis.

ecgHRVtime

HRV Time-Domain Metrics

Description

Compute standard heart rate variability (HRV) time-domain metrics from RR interval data. Calculates SDNN, RMSSD, pNN50, mean RR interval, and mean heart rate for each channel.

Usage

```
ecgHRVtime(rr)
```

Arguments

rr A data.frame with columns channel, rr_ms, and time_sec, as returned by [ecgRRintervals](#).

Value

A data.frame with one row per channel and the following columns:

channel Integer channel index.

mean_rr Mean RR interval in milliseconds.

sdnn Standard deviation of all RR intervals (ms), reflecting overall HRV.

rmssd Root mean square of successive RR interval differences (ms), reflecting short-term vagal modulation.

pnn50 Percentage of successive RR intervals differing by more than 50 ms.

mean_hr Mean heart rate in beats per minute (60000 / mean_rr).

References

Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996). "Heart rate variability: Standards of measurement, physiological interpretation and clinical use." *Circulation*, 93(5), 1043–1065.

See Also

[ecgRRintervals](#) for computing RR intervals, [ecgHRVfreq](#) for frequency-domain HRV analysis, [ecgHRVnonlinear](#) for nonlinear HRV metrics, [ecgQualityCheck](#) for ectopic beat detection before analysis.

 ecgIntervals

Compute ECG Intervals from Delineation

Description

Calculates standard clinical ECG intervals from the waveform delineation produced by [ecgDelineate](#): PR interval, QT interval, QTc (Bazett correction), QRS duration, and RR interval.

Usage

```
ecgIntervals(delineation, sr)
```

Arguments

delineation	A data.frame as returned by ecgDelineate , with columns channel, beat, r_peak, qrs_onset, qrs_offset, p_peak, t_peak, t_end.
sr	Sampling rate in Hz.

Value

A data.frame with one row per beat and the following columns:

channel Integer channel index (1-based).

beat Integer beat number within the channel.

pr_ms PR interval in milliseconds (P-wave peak to QRS onset), or NA if the P wave was not detected.

qt_ms QT interval in milliseconds (QRS onset to T-wave end), or NA if the T wave was not detected.

qtc_ms Corrected QT interval using Bazett's formula ($QT / \sqrt{RR_sec}$), or NA if QT or RR is unavailable.

qrs_ms QRS complex duration in milliseconds.

rr_ms RR interval in milliseconds to the next beat, or NA for the last beat in each channel.

Returns a zero-row data.frame with the same column structure if no beats are present.

References

Goldberger, A.L., et al. (2000). "PhysioBank, PhysioToolkit, and PhysioNet: Components of a new research resource for complex physiologic signals." *Circulation*, 101(23), e215–e220. doi:10.1161/01.CIR.101.23.e215

See Also

[ecgDelineate](#) for waveform delineation, [ecgDetectRpeaks](#) for R-peak detection, [ecgRRintervals](#) for RR interval computation.

Examples

```
## Not run:
pe <- make_ecg(n_time = 5000, sr = 500, heart_rate = 72)
peaks <- ecgDetectRpeaks(pe)
delin <- ecgDelineate(pe, peaks)
intervals <- ecgIntervals(delin, samplingRate(pe))
head(intervals)

## End(Not run)
```

ecgQualityCheck

Detect Ectopic Beats in RR Interval Data

Description

Identifies ectopic (abnormal) beats by comparing each RR interval to the local median computed over a sliding window of 5 beats. Beats with deviation exceeding the threshold are marked as ectopic.

Usage

```
ecgQualityCheck(rr, threshold_ms = 300)
```

Arguments

rr A data.frame with columns channel, rr_ms, and time_sec, as returned by [ecgRRintervals](#).

threshold_ms Maximum allowed deviation from local median in milliseconds (default: 300).

Value

The input data.frame with an additional logical column `is_ectopic`.

References

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996). "Heart rate variability: Standards of measurement, physiological interpretation and clinical use." *Circulation*, 93(5), 1043–1065.

See Also

[ecgRRcorrect](#) for correcting detected ectopic beats, [ecgRRintervals](#) for computing RR intervals, [ecgHRVtime](#) for time-domain HRV analysis, [ecgSignalQuality](#) for signal quality assessment.

ecgRRcorrect	<i>Correct Ectopic Beats in RR Interval Data</i>
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Description

Replaces or removes ectopic beats identified by [ecgQualityCheck](#). The "interpolate" method uses linear interpolation from surrounding non-ectopic intervals, while "remove" simply drops ectopic rows.

Usage

```
ecgRRcorrect(rr, method = c("interpolate", "remove"))
```

Arguments

rr	A data.frame with an <code>is_ectopic</code> logical column, as returned by ecgQualityCheck .
method	Correction method: "interpolate" (default) replaces ectopic values with linear interpolation; "remove" drops ectopic rows.

Value

A data.frame with corrected RR intervals. The `is_ectopic` column is removed from the output.

References

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

See Also

[ecgQualityCheck](#) for detecting ectopic beats, [ecgRRintervals](#) for computing RR intervals, [ecgHRVtime](#) for time-domain HRV analysis.

`ecgRRintervals`*Compute RR Intervals from Detected R-Peaks*

Description

Calculates the time intervals between consecutive R-peaks for each channel. The resulting RR interval series is the standard input for all HRV analysis functions in this package.

Usage

```
ecgRRintervals(x, peaks)
```

Arguments

<code>x</code>	A <code>PhysioExperiment</code> object.
<code>peaks</code>	A <code>data.frame</code> of detected peaks as returned by <code>ecgDetectRpeaks</code> , with columns <code>channel</code> , <code>sample</code> , and <code>time_sec</code> .

Value

A `data.frame` with one row per consecutive beat pair and the following columns:

channel Integer channel index (1-based).

rr_ms RR interval in milliseconds (time between successive R-peaks).

time_sec Time of the first beat in each pair (seconds from signal onset).

Returns a zero-row `data.frame` with the same column structure if fewer than two peaks are available.

References

Pan, J. & Tompkins, W.J. (1985). "A real-time QRS detection algorithm." *IEEE Transactions on Biomedical Engineering*, 32(3), 230–236. doi:[10.1109/TBME.1985.325532](https://doi.org/10.1109/TBME.1985.325532)

See Also

[ecgDetectRpeaks](#) for R-peak detection, [ecgHRVtime](#) for time-domain HRV metrics, [ecgHRVfreq](#) for frequency-domain HRV analysis, [ecgQualityCheck](#) for ectopic beat detection.

Examples

```
## Not run:
pe <- make_ecg(n_time = 5000, sr = 500, heart_rate = 60)
peaks <- ecgDetectRpeaks(pe)
rr <- ecgRRintervals(pe, peaks)
head(rr)

## End(Not run)
```

ecgSampleEntropy *Sample Entropy of RR Intervals*

Description

Computes sample entropy (SampEn) from RR interval data. Sample entropy measures the regularity or predictability of a time series. Lower values indicate more regular (predictable) signals, while higher values indicate more complex (irregular) signals.

Usage

```
ecgSampleEntropy(rr, m = 2L, r_factor = 0.2)
```

Arguments

rr A data.frame with columns channel, rr_ms, and time_sec, as returned by [ecgRRintervals](#).

m Embedding dimension (default: 2). Length of template patterns to compare.

r_factor Tolerance factor (default: 0.2). The tolerance r is computed as $r_factor * sd(rr_ms)$.

Value

A data.frame with one row per channel and the following columns:

channel Integer channel index.

sample_entropy Sample entropy value (nats). Lower values indicate more regular signals; higher values indicate more complex signals. NA if the series is too short or constant.

m Embedding dimension used.

r Tolerance threshold (ms) computed as $r_factor * sd(rr_ms)$.

References

Richman, J.S. & Moorman, J.R. (2000). "Physiological time-series analysis using approximate entropy and sample entropy." *American Journal of Physiology-Heart and Circulatory Physiology*, 278(6), H2039–H2049. doi:10.1152/ajpheart.2000.278.6.H2039

See Also

[ecgHRVnonlinear](#) for the combined nonlinear analysis wrapper, [ecgHRVpoincare](#) for Poincare plot descriptors, [ecgDFA](#) for detrended fluctuation analysis.

ecgSignalQuality *Assess ECG Signal Quality Per Channel*

Description

Computes per-channel signal quality metrics for ECG data stored in a PhysioExperiment object. When detected R-peak locations are provided the signal-to-noise ratio is estimated from QRS vs. baseline power; otherwise a variance-based estimate is used.

Usage

```
ecgSignalQuality(x, peaks = NULL, assay_name = NULL)
```

Arguments

x	A PhysioExperiment object with ECG data.
peaks	Optional data.frame of detected R-peaks as returned by ecgDetectRpeaks , with at least columns channel and sample.
assay_name	Name of the assay to use. If NULL the default assay is used.

Value

A data.frame with one row per channel and columns:

channel Integer channel index.

snr_db Signal-to-noise ratio in decibels.

baseline_wander RMS amplitude of the low-frequency drift.

saturation_ratio Fraction of samples within 1\ min or max.

quality_score Composite quality score in the range [0, 1], where 1 indicates excellent quality.

References

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

Shaffer, F. & Ginsberg, J.P. (2017). "An overview of heart rate variability metrics and norms." *Frontiers in Public Health*, 5, 258. doi:10.3389/fpubh.2017.00258

See Also

[ecgDetectRpeaks](#) for R-peak detection, [ecgBaselineCorrect](#) for baseline wander correction, [ecgQualityCheck](#) for ectopic beat detection.

`make_ecg`*Create Simulated ECG PhysioExperiment*

Description

Generates a PhysioExperiment object containing synthetic ECG data with Gaussian-shaped R-peaks at regular intervals. The resulting object is suitable for testing R-peak detection, RR interval computation, and HRV analysis pipelines.

Usage

```
make_ecg(n_time = 5000, n_channels = 1, sr = 500, heart_rate = 72)
```

Arguments

<code>n_time</code>	Number of time points (default: 5000).
<code>n_channels</code>	Number of ECG channels (default: 1).
<code>sr</code>	Sampling rate in Hz (default: 500).
<code>heart_rate</code>	Heart rate in beats per minute (default: 72).

Value

A PhysioExperiment object with a single "raw" assay containing the simulated ECG signal.

References

Pan, J. & Tompkins, W.J. (1985). "A real-time QRS detection algorithm." *IEEE Transactions on Biomedical Engineering*, 32(3), 230–236. doi:[10.1109/TBME.1985.325532](https://doi.org/10.1109/TBME.1985.325532)

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

See Also

[make_ecg_irregular](#) for ECG with ectopic beats, [make_ecg_pqrst](#) for ECG with full PQRST morphology, [make_ecg_noisy](#) for ECG with noise artifacts, [ecgDetectRpeaks](#) for R-peak detection.

Examples

```
pe <- make_ecg(n_time = 5000, sr = 500, heart_rate = 72)
pe
```

make_ecg_irregular *Create Simulated ECG with Irregular R-R Intervals*

Description

Generates a `PhysioExperiment` object containing synthetic ECG data with irregular beat timing. Every 5th beat is premature (60\ interval), followed by a compensatory pause (140\ Useful for testing ectopic beat detection and RR interval correction.

Usage

```
make_ecg_irregular(n_time = 5000, sr = 500, heart_rate = 72)
```

Arguments

n_time	Number of time points (default: 5000).
sr	Sampling rate in Hz (default: 500).
heart_rate	Base heart rate in beats per minute (default: 72).

Value

A `PhysioExperiment` object with a single "raw" assay containing the simulated ECG signal with irregular beats.

References

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996). "Heart rate variability: Standards of measurement, physiological interpretation and clinical use." *Circulation*, 93(5), 1043–1065.

See Also

[make_ecg](#) for regular ECG data, [ecgQualityCheck](#) for ectopic beat detection, [ecgRRcorrect](#) for ectopic beat correction, [ecgRRintervals](#) for RR interval computation.

Examples

```
pe <- make_ecg_irregular(n_time = 5000, sr = 500, heart_rate = 72)
pe
```

Description

Generates a `PhysioExperiment` object containing synthetic ECG data contaminated with multiple noise sources: baseline wander (0.3 Hz sinusoidal drift), powerline interference (50 Hz), and broadband Gaussian noise. Useful for testing signal quality assessment, baseline correction, and filtering pipelines.

Usage

```
make_ecg_noisy(  
  n_time = 5000,  
  n_channels = 1,  
  sr = 500,  
  heart_rate = 72,  
  baseline_amp = 0.3,  
  powerline_amp = 0.1,  
  noise_sd = 0.15  
)
```

Arguments

<code>n_time</code>	Number of time points (default: 5000).
<code>n_channels</code>	Number of ECG channels (default: 1).
<code>sr</code>	Sampling rate in Hz (default: 500).
<code>heart_rate</code>	Heart rate in beats per minute (default: 72).
<code>baseline_amp</code>	Amplitude of baseline wander in arbitrary units (default: 0.3).
<code>powerline_amp</code>	Amplitude of 50 Hz powerline noise (default: 0.1).
<code>noise_sd</code>	Standard deviation of broadband Gaussian noise (default: 0.15).

Value

A `PhysioExperiment` object with a single "raw" assay containing the noisy ECG signal.

References

- Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.
- Shaffer, F. & Ginsberg, J.P. (2017). "An overview of heart rate variability metrics and norms." *Frontiers in Public Health*, 5, 258. doi:10.3389/fpubh.2017.00258

See Also

[make_ecg](#) for clean ECG data, [ecgSignalQuality](#) for signal quality assessment, [ecgBaselineCorrect](#) for baseline wander removal, [ecgDetectRpeaks](#) for R-peak detection.

Examples

```
pe <- make_ecg_noisy(n_time = 5000, sr = 500)
pe
```

make_ecg_pqrst	<i>Create Simulated ECG with PQRST Morphology</i>
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Description

Generates a `PhysioExperiment` object containing synthetic ECG data with physiologically realistic P, Q, R, S, and T wave components. Returns both the `PhysioExperiment` and a `data.frame` of known fiducial points for validation testing of waveform delineation algorithms.

Usage

```
make_ecg_pqrst(  
  n_time = 10000,  
  n_channels = 1,  
  sr = 500,  
  heart_rate = 72,  
  noise_sd = 0.02  
)
```

Arguments

<code>n_time</code>	Number of time points (default: 10000, i.e., 20 seconds at 500 Hz).
<code>n_channels</code>	Number of ECG channels (default: 1).
<code>sr</code>	Sampling rate in Hz (default: 500).
<code>heart_rate</code>	Heart rate in beats per minute (default: 72).
<code>noise_sd</code>	Standard deviation of baseline noise (default: 0.02).

Value

A list with two components:

pe `PhysioExperiment` object with the simulated ECG signal.

fiducials A `data.frame` with columns: `beat`, `r_peak`, `p_peak`, `q_point`, `s_point`, `t_peak`, `qrs_onset`, `qrs_offset` (all in sample indices).

References

Goldberger, A.L., et al. (2000). "PhysioBank, PhysioToolkit, and PhysioNet: Components of a new research resource for complex physiologic signals." *Circulation*, 101(23), e215–e220. doi:10.1161/01.CIR.101.23.e215

Clifford, G.D., Azuaje, F. & McSharry, P.E. (2006). *Advanced Methods and Tools for ECG Data Analysis*. Artech House.

See Also

[make_ecg](#) for basic ECG data, [ecgDelineate](#) for PQRST waveform delineation, [ecgIntervals](#) for computing clinical ECG intervals, [ecgDetectRpeaks](#) for R-peak detection.

Examples

```
result <- make_ecg_pqrst(n_time = 10000, sr = 500, heart_rate = 72)
pe <- result$pe
fiducials <- result$fiducials
head(fiducials)
```

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